Estimating the complete ground reaction forces with pressure insoles in walking

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Conflict of interest

Editor of Journal of Biomechanics,

REF: Submission of manuscript “Estimating complete ground reaction force with pressure insoles in walking”

The authors would like to declare no conflict of interest in the above mentioned submission of manuscript to the Journal of Biomechanics.

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Cover letter

Editor of Journal of Biomechanics,

REF: Submission of manuscript “Estimating complete ground reaction force with pressure insoles in walking”

The authors would like to declare that this piece of work is neither published nor submitted for consideration of publication elsewhere except as an abstract. The manuscript is submitted as a “Short Communication”. We declare that each author has been involved in the design of the study, interpretation of the data, and writing of the manuscript and that each of the authors has read and concurs with the content in the manuscript. We declare the originality of concept and execution of this paper.

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Estimating the complete ground reaction forces with pressure insoles in walking

Abstract

This study presented a method to estimate the complete ground reaction forces from pressure insoles in walking. Five male subjects performed ten walking trials in a laboratory. The complete ground reaction forces were collected during a right foot stride by a force plate at 1000 Hz. Simultaneous plantar pressure data were collected at 100 Hz by a pressure insole system with 99 sensors covering the whole plantar area. Stepwise linear regressions were performed to individually reconstruct the complete ground reaction forces in three directions from the 99 individual pressure data until redundancy among the predictors occurred. An additional linear regression was performed to reconstruct the vertical ground reaction force by the sum of the value of the 99 pressure sensors. Five other subjects performed the same walking test for validation. Estimated ground reaction forces in three directions were calculated with the developed regression models, and were compared with the real data recorded from force plate. Accuracy was represented by the correlation coefficient and the root mean square error. Results showed very good correlation in anterior-posterior (0.928) and vertical (0.989) directions, and reasonable correlation in medial-lateral direction (0.719). The root mean square error was about 12%, 5% and 28% of the peak recorded value. Future studies should aim to generalize the methods or to establish specific methods to other subjects, patients, motions, footwear, and floor conditions. The method gives an extra option to study an estimation of the complete ground reaction forces in any environment without the constraints from the number and location of force plates.

Keywords: Kinetics, plantar pressure, gait, biomechanics
Introduction

Ground reaction forces are often investigated in gait biomechanics studies (Kitaoka et al., 2006). However, the measurement is often restricted by the number and the location of force plates. In attempt to measure vertical and shear ground reaction forces without such restriction, different devices were developed, such as a thin layer of strain gauge transducer (Davis et al., 1998) or piezoelectric copolymer film (Razian et al, 2003), and instrumented shoe with two sensors mounted beneath the forefoot and rearfoot (Liedtke et al., 2007; Schepers et al, 2007). However, these devices were limited to its specific purpose and thus were not readily available for other researchers. For example, although the instrumented shoe with two external mounted sensors beneath the forefoot and rearfoot (Liedtke et al., 2007; Schepers et al, 2007) could measure complete shear and vertical ground reaction force, the external device lifts the shoe sole and separates it from the ground by the two mounting frames. This changes the original interface between shoe-sole and the ground to an interface between the mounting frames and the ground, and could probably alter the friction between the contact interface. Moreover, it may increase the height of the effective sole and also the weight of the sole. For the shoe with an instrumented insole with strain gauge transducer or piezoelectric copolymer film, the high cost of the sensor resulted in the use of a limited number of sensors, and thus an inadequate coverage of the whole plantar region. For example, the complete ground reaction forces could only be measured in the forefoot region with 16 sensors in Davis’s device (1998), and at only four selected regions (heel, toe, 1st and 5th metatarsal head) in Razian’s device (2003).

Recently, Forner-Cordero and coworkers (2004) developed a method to calculate
complete ground reaction forces during gait by incorporating pressure insole data and
kinematics data in a validated calculation algorithm. The kinematics data provided
information for the transformation between the insole reference frame and the global
reference frame, which facilitated the subsequent calibration of the vertical ground
reaction force and the computation of the complete ground reaction force. Although
the results were excellent, the method relied on kinematics data from a motion capture
system and thus was still not readily applicable in outdoor environment, as it often
requires substantial effort in calibrating outdoor environment for kinematics
measurement. Moreover, the vision-based motion measurement systems often have a
limited measurement volume as dictated by the vision field of the cameras. Another
previous study suggested that the plantar pressure distribution was related to the shear
ground reaction force (Savelberg and de Lange, 1999). The result suggested a
mechanical relation between plantar pressure and shear ground reaction force, which
led to the current attempt to develop a method and test the feasibility to estimate the
complete ground reaction forces with only pressure insole data during walking in a
small group of subjects. As the new method is free from the restrictions of force plate
and motion capture system, it is suitable for rapid on-field measurement in all settings,
provided that the subsequent future studies to generalize the method on other subject
groups are successful.

Method

Calibration test
Five right-legged male subjects (age = 23.0 ± 3.0 yr, height = 1.72 ± 0.03 m, body
mass = 65.1 ± 9.7 kg, foot length = 255-260 mm) wore a pair of cloth sport shoes
(Fong et al., 2007) and performed ten trials of walking at their natural cadence on a
10-metre walking path in a gait laboratory. The university ethics committee approved
the study. In each trial, the subject stepped on a force plate (Advanced Mechanical
Technology Inc., USA) located at the middle of the walking path with their right foot.
The complete ground reaction forces for the right foot were sampled by the force plate
at 1000 Hz. A pair of pressure insoles (Novel Pedar model W, Germany) was inserted
in the shoes for the simultaneous measurement of plantar pressure at 100 Hz. There
were 99 sensors in each insole, covering the whole plantar area, and recording
pressure data with a resolution of 2.50 kPa.

The force plate data and the plantar pressure data for the right foot were trimmed for
one complete stride, from the moment of take off before the foot strike on the force
plate, until the next take off from the force plate. The first moment of take off before
the foot strike on the force plate was identified by the null plantar pressure value as
recorded by the pressure insoles. The second moment of take off from the force plate
was identified when the vertical ground reaction force as recorded by the force plate
drop beneath 10N. The force plate data were re-sampled to have data point in every
0.01s to match the sampling frequency of the pressure data. Data from all trials and all
subjects were pooled together for stepwise linear regression analysis to reconstruct the
value of the ground reaction force in three directions (anterior-posterior, Fx_fp;
medial-lateral, Fy_fp; vertical, Fz_fp; unit = N) by the value of the 99 pressure
sensors (P1, P2, ..., P99, unit = kPa). In each stepwise regression analysis, predictors
were added to the regression models until the inclusion of the next predictor showed
redundancy or multicollinearity, as indicated by a tolerance value of less than 0.20 and
a variance-inflation factor value of more than 4. An additional linear regression
analysis was conducted to reconstruct the vertical ground reaction force by the sum of
the value of the 99 pressure sensors (PSum, unit = kPa).
Another group of five right-legged male subjects (age = 23.8 ± 3.3 yr, height = 1.74 ± 0.03 m, body mass = 65.4 ± 7.3 kg, foot length = 255-260 mm) participated in the validation test. Independent t-tests showed that the two groups of subjects did not differ in age, height and body mass. The subjects performed the walking test with the same procedure with the calibration test. Beside the complete ground reaction forces recorded by the force plate, the estimated ground reaction forces were also calculated by inputting the pressure value of the selected sensor locations to the regression models developed in the calibration test. Correlation coefficient (R) and the root mean square error (RMS error) were computed between the data measured with force plates and estimated from the regression models, for the comparison of accuracy with Forner Cordero’s method (2004).

Results

Table 1 shows the results of regression analysis, which included the equations to estimate the value of the complete ground reaction forces recorded from the force plate, and the amount of explained variance (Adjusted R²) of the regression models. Figure 1 shows the locations of the sensors included in each regression model employing individual pressure sensor value as predictors. Four, six and four sensors among the total 99 sensors were required for the estimation of the ground reaction force for anterior-posterior, medial-lateral and vertical directions respectively, as shown in Figure 1. The sum of the value of the 99 pressure sensors (PSum) was also found to be relevant in reconstructing the vertical ground reaction force.

The accuracy of the estimation was also shown in Table 1, as indicated by the correlation and the RMS error between the real and estimated data. Corresponding
results from Forner Cordero’s study (2004) are also included for comparison. Figure 2 shows the pattern and the absolute error of the real and estimated data of a complete stride trial with an average accuracy among the 50 trials in the validation test. The accuracy of the results was very good in the estimation of ground reaction force in anterior-posterior and vertical directions, as indicated by a very high correlation between the real and estimated data (0.928 and 0.989). The RMS error was 27.41N and 45.79N respectively, which was only about 12% and 5% of their peak values. The estimation in medial-lateral direction was fair, with a correlation value of 0.719 between the real and estimated data. The RMS error was 11.71N, which was as much as 28% of the peak value. In general, the pattern and accuracy of the results of this study were similar but slightly inferior to that from Forner Cordero’s study (2004), as indicated by lower correlations, greater RMS errors and same deficiency in estimating the ground reaction force in medial-lateral direction.

The pattern of the estimated data was similar to that of real data, as shown in a selected trial with average accuracy in Figure 2. The solid line shows the pattern of the real ground reaction force data as measured by the force plate (Fx_fp, Fy_fp, Fz_fp), and the dotted line showed the estimated data calculated from the regression models shown in Table 1 (Fx_est, Fy_est, Fz_est, Fz_est_sum). At the time right after the foot strike, the estimation of the peaks was found to be very accurate. The estimated values were about 95%-105% of the real data in all three directions. However, the plots of absolute error suggested that the largest error occur right after foot strike and just before take off – this implied that the estimation was even more accurate during the mid-stance period. However, at the period just before take off, relatively larger errors were found in both anterior-posterior and medial-lateral components.
Discussion

In the estimation of the vertical force, four critical sensor locations (P1, P18, P71, P74) or the sum of the value of the 99 pressure sensors could both work well with comparable accuracy. The four locations spread around the plantar region, with two at the metatarsal region and two at the rearfoot region. In the estimation of anterior-posterior shear force, the mechanical relation between plantar pressure and shear ground reaction force was somewhat reflected by the position of the essential pressure sensors for the estimation. The locations P13 and P60 contributed negatively to the estimated value – when they were on, especially during the heel strike period and the weight acceptance period by midfoot, the ground reaction force was in a rather backward direction. The locations P90 and P97 around the hallux region contributed positively. They were on, especially at the propulsion and take off period, when the hallux was almost the only contact region of the foot and the ground. The corresponding ground reaction force was in the anterior direction for propulsion. This also reflected the characteristics of heel-toe walking which lead to this unique mechanical relation between plantar pressure and shear ground reaction force in anterior-posterior direction.

This study presented a feasible method to estimate complete ground reaction forces with pressure insole data during walking, however, the current findings are limited to a small homogenous group of male young subjects only. Future studies should aim to generalize the methods, or to establish specific methods to other subjects, patients, motions, footwear, and floor conditions, etc. Although the method presented in the current study is slightly inferior to that presented by Forner Cordero and coworkers (2004), it does not require a motion capture system for the calculation of complete
ground reaction force. Therefore, if the level of accuracy is adequate, or if the inferior  
accuracy could be tolerated, the current method is readily available for measurement  
in any environment out of the laboratory. Considering the good and reasonable  
accuracy and the possible rapid application in any environment, the method presented  
in this study should give an extra option to study complete ground reaction forces  
with less constraint from the number and location of force plates. Before the future  
studies to generalize the methods to other conditions, we suggest performing  
calibration and measurement on the same group of subject with the same type of  
shoes. The method presented could be implemented to the original pressure insole  
system for immediately estimation of the complete ground reaction forces during data  
collection, and could be useful for real-time analysis for sport biomechanics tests  
which requires immediate display of data and reports.

Conclusion

This study presented a feasible method to estimate complete ground reaction forces  
with pressure insole data during walking, which eliminates the constraint introduced  
by number and location of force plates in biomechanics studies. The results were with  
very good in estimating anterior-posterior and vertical ground reaction force, and with  
reasonable accuracy in estimating that in medial-lateral direction. The method can  
serve as an extra option in measuring complete ground reaction forces in any  
environment out of the laboratory without using force plates.

Acknowledgement

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Innovation and Technology Commission, Hong Kong Special Administrative Region
References


Dear Professor Chan,

Thank you for your submission to the Journal of Biomechanics. After considering the enclosed reviews from our referees, I regret to inform you that our referee panel recommends against publication of your manuscript in its current form, although a revised manuscript may be resubmitted and considered after further review.

If you choose to submit a revised manuscript, please provide a list of points of how you have responded to the reviewers' suggestions.

To submit a revision, go to http://ees.elsevier.com/bm/ and log in as an Author. You will see a menu item called Submission Needing Revision. You will find your submission record there. Please update accordingly and submit your revised manuscript.

We look forward to receiving your revised manuscript.

Yours sincerely,

Dr Rik Huiskes
Editor in Chief
Journal of Biomechanics
Reviewers' comments:

Reviewer #1: The authors have addressed satisfactorily the proposed questions. The manuscript has improved significantly. However, there are still some minor errors, mostly grammar errors or ambiguous sentences that must be corrected. Please, revise the text for grammatical correctness.

It is used through the text "complete ground reaction force", although in general it is usual to name them as "the complete ground reaction forces".

>>> Revised accordingly.

Line 32: please correct "...including a thin layer..." or even better, "...consisting of a thin layer..."

>>> The paragraph lists some different devices, so it read “including a thin layer of strain gauge transducer (Davis et al., 1998) or piezoelectric copolymer film (Razian et al, 2003), and instrumented shoe with two sensors mounted beneath the forefoot and rearfoot (Liedtke et al., 2007; Schepers et al, 2007)”. The term “including” is revised to be “such as” in the revised manuscript.

Line 80: This description is somewhat ambiguous. Were the authors using two force plates? Otherwise, they only measured the complete ground reaction forces during single stance. Please, clarify this point. If the forces measured are not complete (in 3-D but also under both feet) then correct the text.

>>> Only one force plate is used, and the complete ground reaction forces in 3D for only the right foot was recorded and analyzed. The left foot did not step on the same force plate. The sentence is revised as “The complete ground reaction forces for the right foot were sampled by the force plate at 1000 Hz” (Line 81).

In line 86 it is said that the data are trimmed for one complete stride. Is this correct? A stride is defined between two consecutive ground contacts with the same foot. This would imply the need of up to three force plates to record a complete stride. From the explanations provided in the text it seems that the authors only measured the complete forces under one foot. Please, let clear in the text which forces you are referring to.

>>> The first moment of take off before the foot strike on the force plate was identified by the null plantar pressure value as recorded by the pressure insoles. The second moment of take off from the force plate was identified when the vertical ground reaction force as recorded by the force plate drop beneath 10N. This information is added in the revised manuscript (Line 89-93).
Line 172 and line 193 it is said that "This study presented a good feasibility to estimate..." Please, explain better, a good feasibility method to estimate?

>>> Revised accordingly to “a feasible method to estimate…”.

Reviewer #2: My comments have been processed adequately
Abstract

This study presented a method to estimate complete ground reaction force from pressure insoles in walking. Five male subjects performed ten walking trials in a laboratory. Complete ground reaction force was collected during a right foot stride by a force plate at 1000 Hz. Simultaneous plantar pressure data were collected at 100 Hz by a pressure insole system with 99 sensors covering the whole plantar area. Stepwise linear regressions were performed to individually reconstruct the complete ground reaction force in three directions from the 99 individual pressure data until redundancy among the predictors occurred. An additional linear regression was performed to reconstruct the vertical ground reaction force by the sum of the value of the 99 pressure sensors. Five other subjects performed the same walking test for validation. Estimated ground reaction forces in three directions were calculated with the developed regression models, and were compared with the real data recorded from force plate. Accuracy was represented by the correlation coefficient and the root mean square error. Results showed very good correlation in anterior-posterior (0.928) and vertical (0.989) directions, and reasonable correlation in medial-lateral direction (0.719). The root mean square error was about 12%, 5% and 28% of the peak recorded value. Future studies should aim to generalize the methods or to establish specific methods to other subjects, patients, motions, footwear, and floor conditions. The method gives an extra option to study complete ground reaction forces in any environment without the constraints from the number and location of force plates.
**Figure legends**

Figure 1 – Location of the sensors (in right foot) required in the three regression models (in grey).

Figure 2 – Pattern and the absolute error of real and estimated complete ground reaction force data in a selected trial of a complete stride, from the previous take off (time = -0.31s), foot strike (time = 0.00s) to the next take off (time = 0.53s), as shown by the dotted lines.
Figure 1
Click here to download high resolution image
Table 1 – Results of regression analysis and the comparison of accuracy with Forner Cordero’s study.

<table>
<thead>
<tr>
<th>Force direction</th>
<th>Regression models</th>
<th>Adjusted $R^2$</th>
<th>R</th>
<th>RMS Error (N)</th>
<th>Forner Cordero’s study</th>
</tr>
</thead>
<tbody>
<tr>
<td>Anterior-posterior (Fx_fp)</td>
<td>$F_x_{\text{est}}(N) = 1.364 - 32.045 \times (P13) + 4.452 \times (P90) + 4.847 \times (P97) - 2.796 \times P60$</td>
<td>0.904</td>
<td>0.928</td>
<td>27.41</td>
<td>0.977-0.979</td>
</tr>
<tr>
<td>Medial-lateral (Fy_fp)</td>
<td>$F_y_{\text{est}}(N) = 2.622 - 3.158 \times (P60) - 8.734 \times (P33) - 1.508 \times (P84) - 1.654 \times (P22) + 2.261 \times (P1) - 2.310 \times P19$</td>
<td>0.764</td>
<td>0.719</td>
<td>11.71</td>
<td>0.778-0.818</td>
</tr>
<tr>
<td>Vertical (Fz_fp)</td>
<td>$F_z_{\text{est}}(N) = -18.938 + 8.001 \times (P74) + 31.446 \times (P18) + 30.836 \times (P71) + 15.150 \times (P1)$</td>
<td>0.975</td>
<td>0.989</td>
<td>45.79</td>
<td>0.995-0.997</td>
</tr>
<tr>
<td></td>
<td>$F_z_{\text{est _ sum}}(N) = -31.132 + 1.696 \times (P\text{Sum})$</td>
<td>0.985</td>
<td>0.992</td>
<td>38.43</td>
<td>0.995-0.997</td>
</tr>
</tbody>
</table>

(* Unit: force in N, pressure in kPa. PX is the value of pressure of the sensor number X. PSum is the value of the sum of the pressure values of the 99 sensors.*)